#### **1** Investigation of graphene oxide/mesoporous silica supports for enhanced electrochemical

#### 2 stability of enzymatic electrodes

- 3 Şevval Kaya<sup>a</sup>, Veli Şimşek<sup>a,b</sup>, Samet Şahin<sup>c,d,\*</sup>
- 4 <sup>a</sup> Bilecik Seyh Edebali University, Department of Biotechnology, 11100 Bilecik, Turkey
- <sup>b</sup> Bilecik Seyh Edebali University, Faculty of Engineering, Department of Chemical Engineering, 11100 Bilecik,
- 6 Turkey
- 7 <sup>c</sup> Bilecik Seyh Edebali University, Faculty of Engineering, Department of Bioengineering, 11100 Bilecik, Turkey
- <sup>d</sup> School of Engineering, Lancaster University, Lancaster LA1 4YW, UK
- 9 \*Corresponding Author: Samet Şahin (s.sahin@lancaster.ac.uk)
- 10

## 11 Abstract:

12 Mesoporous silica materials (MSMs) are widely used materials in many applications due to their diverse pore structures. However, the electrical conductivity of MSMs is poor which 13 limits their use in electrochemical applications. In this study, widely used MSMs of different 14 structural properties such as MCM-41, MCM-48, SBA-15, and SBA-16 were synthesized and 15 16 reinforced with graphene oxide (GO) to obtain conductive composite supports for enzyme immobilization. MSMs were first synthesized using a hydrothermal method and characterized 17 by Fourier-transform infrared spectroscopy, X-ray crystallography, scanning electron 18 microscopy/energy dispersive X-ray, and MAPPING techniques. Aqueous dispersion of 19 GO:MSM composites were prepared with as-synthesized materials and coated on screen-20 printed electrodes (SPE). The best composites were chosen based on their electroanalytical 21 performance. Glucose oxidase (GOx) was then immobilized on modified SPEs using a simple 22 drop-casting method to produce enzymatic electrodes. The electroanalytical performance of the 23 enzymatic electrodes was investigated using different glucose concentrations to demonstrate 24 25 biocatalytic activity. Stability tests were performed using intraday and interday measurements which revealed that SPE/GO:MCM-41/GOx electrode showed a more stable performance (3-26 27 folds) than SPE/GO/GOx electrode. This study presents an investigation of MSM mixed with GO in enzymatic electrochemical systems providing insight into the use of such materials to 28 29 preserve enzyme activity.

Keywords: Mesoporous silica materials (MSMs), graphene oxide, glucose oxidase,
hydrothermal method, electrochemistry

- 32
- 33

#### 35 **1. Introduction**

Mesoporous silica materials (MSMs) have widely been used as adsorbents, thin films, low-k materials, nanowires, and catalysts due to their large specific surface areas and pore sizes ranging from 2 to 50 nm [1]. Some of the most common MSMs known in the market are SBA-15 and M41S-family due to their high surface area, large pore volume, regular pore distribution, and flexible synthesis conditions [2-4]. There are different variations of MSMs available with various pore shapes and sizes of both families providing opportunities in catalysis, drug delivery and imaging applications.

43 MSMs with diverse pore configurations include MCM-41 (hexagonal pores), MCM-48 (cubic 44 pores), and MCM-50 (unstable lamellar pores) [5]. Furthermore, well-known MSMs have space 45 groups of p6mm (MCM-41), Ia3d (MCM-48), p6mm (SBA-15), and Im3m (SBA-16) [6]. Silica materials have a high number of silanol groups on their surface, we can readily adjust the 46 47 physicochemical nature of the surface through the functionalization process. On the other hand, MSMs have a large surface area and a high pore volume, which means they have a high loading 48 49 capacity and are unique prospects for various applications [7] such as biomaterials [8], catalyst [9], adsorbent [10], sensor [11], and drug delivery [12]. 50

In the M41S family, the pores of MCM-41 type catalysts are in a two-dimensional hexagonal 51 structure, while the pores of MCM-48 are in a three-dimensional cubic structure [13,14]. SBA-52 15, on the other hand, has high thermal stability and a wheat chain structure and SBA-16 is 53 considered the most interesting mesothelium among SBA-type silica materials and is widely 54 used in the field of biomaterials due to its spherical morphology [15,8]. Different methods are 55 used in the synthesis of MSMs such as impregnation, precipitation/co-precipitation, sol-gel, ion 56 exchange, thermal fusion, solid-liquid leaching, and wet impregnation [16]. However, 57 depending on the thermal strength and the amount of material obtained after synthesis, the 58 59 hydrothermal synthesis method is widely used in the synthesis of silica-derived mesoporous 60 materials since it can eliminate the use of high-grade materials.

Silica-based materials are known as poor electrical conductors, but they have been utilized in electrochemical systems. There are several examples of the way silica-based materials were employed in these systems such as deposited on conductive electrode surfaces or as thin films, manufactured as metal or carbon composites, and dispersed into conductive composites [17]. Therefore, they can be utilized as an immobilization matrix for selective ligands,

34

electrocatalysts, metal particles, and enzymes [18]. There are also examples of MSMs 66 reinforced with carbon-based materials such as carbon nanomembranes [19] and mesoporous 67 carbon [20] mainly for capacitor applications. This potential of MSMs in electrochemical 68 systems opened up possibilities for their use in immunological sensors, aptasensors, and 69 enzymatic biosensors [21-23]. Such systems can offer a variety of opportunities for different 70 applications such as diagnosis of bacterial infections, cancer therapy, cancer detection, 71 detection of heavy metals, contaminated food detection, the detection of viruses, and enzymatic 72 73 biosensors [22].

74 The use of MSMs in enzymatic biosensing is a promising application since the critical aspects 75 of enzymatic systems can be supported by MSMs due to their critical properties. MSMs are 76 shown to be effective in preserving the activity of enzymes due to their porous structure 77 providing a protective environment for the enzymes [24,25]. Furthermore, the high specific pore volume of silica particles can accommodate high enzyme loadings, thus resulting in high 78 current density from enzymatic electrochemical reactions. There are several studies 79 80 demonstrating the use of MSMs in enzymatic electrochemical systems for the detection of cholesterol [26], catechol [27], ethanol [28], hydrogen peroxide [29], lactic acid [30], uric acid 81 [31], and glucose [28]. Different composites were prepared to increase the conductivity of the 82 MSM-modified electrodes and to retain the enzyme activity for glucose detection such as gold 83 nanoparticles [32,33], Prussian-blue [34], Nafion [35,36], and single-walled carbon nanotubes 84 [37]. 85

86 There are a few studies in the literature demonstrating the use of enzyme-incorporated MSMs for biosensing applications using glucose oxidase (GOx) and laccase. In these studies, Yusan 87 et. al. demonstrated that nanoparticle selenium incorporated MCM-41 could be very effective 88 in retaining enzyme activity [38]. On the other hand, another study by Tvorynska et al. also 89 showed that the MCM-41 incorporated sensor was found to be the most stable sensor 90 configuration for laccase-based biosensors [39]. Most of the studies utilizing MSMs for 91 enzymatic biosensors showed promising performance and good stability, yet there is still a need 92 for comprehensive and systematic studies to demonstrate the effect of the conducting composite 93 materials and the performance of the MSMs on retaining enzyme activity fundamentally. 94

Herein, four different MSMs from two different types (M41S and SBA) were first synthesized
using a hydrothermal method. Then, graphene oxide (GO)-MSM composites were prepared as
dispersions of as-synthesized material of optimized amounts into a conductive aqueous GO
matrix. Screen-printed electrodes (SPEs) were modified with different material loadings of the

99 prepared composite dispersions and electrochemically characterized using voltammetry and 100 amperometry. The electroanalytical performance of the GOx immobilized electrodes was 101 investigated in terms of the sensitivity and stability of the enzyme. As a result, this study aims 102 to present a comprehensive investigation of the performance of MSMs reinforced with GO in 103 enzymatic electrochemical applications for the first time in the literature. Therefore, it can 104 provide insight into the use of MSMS as additives to carbon-modified electrochemical 105 electrodes (such as graphene, nanotubes, graphite, etc.) to retain enzyme activity.

### 106 **2. Experimental**

## 107 **2.1. Materials**

Pluronic p 123, Pluronic p 127, and the chemicals used in electrochemical studies were obtained
at analytical grade from Sigma-Aldrich. Cetyltrimethylammonium bromide (CTMAbr),
tetraethyl orthosilicate, (TEOS), and sodium silicate were obtained from Merck.

### 111 2.2. Synthesis and characterization of mesoporous silica

112 The synthesis of MCM-41, SBA-15, MCM-48, and SBA-16 was carried out using the hydrothermal method according to the literature [40-43]. Briefly, the surfactant was dissolved 113 114 at different temperatures and durations (MCM-41 and MCM-48; 30°C, 2-6 hours, SBA-15; 40°C, 2 hours, SBA-16; 38°C, 2 hours) using a magnetic stirrer (Elektro-mag, Turkey) 115 following by filtration and drying. The synthesis is then completed with the calcination process 116 at different temperatures to remove impurities in the structure of materials (MCM-41 and 117 MCM-48: 550°C and 6 hours, SBA-15 and SBA-16: 540°C and 5 hours). Although the same 118 hydrothermal synthesis method is used in the synthesis of these mesoporous materials, different 119 chemicals are used as surfactants (CTMAbr, pluronic p 123, and pluronic p 127) and silica 120 sources (TEOS and sodium silicate). 121

Fourier-transform infrared spectroscopy (FT-IR) analyses of mesoporous materials were 122 performed using the Perkin Elmer IR USA (Attenuated Total Reflectance (ATR) technique) 123 device between 380 and 4000 cm<sup>-1</sup>. The Panalytical Empryan HT (Netherlands) instrument was 124 125 used to perform X-ray crystallography (XRD) analyses to determine the structural phases of mesoporous materials using CuK (= 1.540) radiation, 0.066 step size (sensitivity), 30 V 126 (tension), 40 kV (current), and  $0^{\circ} < 2\Theta < 70^{\circ}$  range. The surface morphologies of the samples 127 were analyzed using scanning electron microscopy/energy dispersive X-ray (SEM/EDX, Zeiss 128 129 SUPRA V40, Germany) analysis. In addition, the MAPPING analysis method was used to determine the distributions of C and Si elements in the structure of the catalyst sample. 130

### 131 **2.3. Electrode preparation and characterization**

All electrochemical experiments were carried out at 23±1 °C using Ivium Potentiostat (Ivium 132 Technologies, Netherlands) and carbon SPE (Model: Dropsens DRP-X1110 with a carbon 133 working electrode surface area of 0.059 cm<sup>2</sup>, obtained from Metrohm AG, Switzerland). Carbon 134 and silver paste electrodes were used as the counter, and reference electrodes, respectively. 135 SPEs were pre-treated using linear sweep voltammetry (LSV) in a solution containing 0.1 M 136 KCl to remove impurities on the working electrode surface and obtain reproducible results 137 before any experiments [44]. Aqueous dispersions of GO (1 mg/mL, Ultra-pure water, 18.2 138 139 MΩ-cm, 4-10% edge oxidized exfoliated graphene nanoplatelets, Sigma-Aldrich) and GOmesoporous silica mixtures with different mass ratios (1:1, 1:1.5, and 1:2) were prepared and 140 sonicated (Bandelin RK 100 H, Germany) until homogenous mixtures were obtained. Then, the 141 working electrode of the SPEs was drop-coated until a material loading of 0.15 mg/cm<sup>2</sup> was 142 143 achieved [45]. This value was chosen due to physical constraints of the working electrode surface area and above this level, the coating failed. The coated electrodes with different 144 145 material ratios were then electrochemically characterized using cyclic voltammetry (CV, 50 mV/s) in a solution containing 2 mM K<sub>3</sub>Fe(CN)<sub>6</sub>/K<sub>4</sub>Fe(CN)<sub>6</sub> redox couple in 0.1 M KCl. Bare 146 electrode (BE) and GO-only coated SPE were also tested as control experiments. The optimal 147 GO to mesoporous silica amount ratio was chosen based on the anodic and cathodic current 148 changes in CV experiments. 149

## 150 **2.4.** Enzyme immobilization and electrochemical glucose oxidation

First, drop-coating 1 µL of ethanoic Nafion solution (0.05 % w/w in ethanol) as a supporting 151 layer and dried at room temperature for 15 mins. Subsequently, drop-coating 1  $\mu$ L of GOx (1, 152 5, and 10 mg/mL in 0.1 M phosphate buffer (PBS), pH 7.4) on Nafion-modified SPEs created 153 an active enzymatic layer for electrochemical glucose oxidation. All prepared electrodes were 154 kept at 4 °C for 24 hours and immersed in PBS for 15 mins following consecutive washing 155 steps at least 3 times to remove weakly adsorbed species before use. The prepared enzymatic 156 157 electrodes were denoted as SPE/GO/GOx, SPE/GO:MCM-41/GOx, SPE/GO:MCM-48/GOx, SPE/GO:SBA-15/GOx, and SPE/GO:SBA-16/GOx. The electrochemical glucose oxidation 158 159 was tested using chronoamperometry (CA) with an applied voltage of 0.14 V for 120 s in 1 mM ferrocene carboxylic acid (FcCOOH, in 0.1 M PBS, pH 7.4) containing 0 and 5 mM glucose. 160 161 The enzyme concentration for the immobilization was also optimized using LSV (5 mV/s) and 162 used for the electrochemical performance tests. All electrochemical tests were conducted with

three independently prepared electrodes unless otherwise stated (N=3 samples). A schematic representation of electrode preparation steps is shown in Fig. 1.



166 Fig. 1. Schematic representation of electrode preparation steps using MSMs

## 167 3. Results and Discussion

165

# 168 **3.1.** Characterization studies of the mesoporous silica materials

Characterizations of the synthesized MCM-48, MCM-41, SBA-16, and SBA-15 were first 169 performed using FT-IR, XRD, and SEM. FT-IR analysis results of silica-derived mesoporous 170 materials showed that Si-O-Si bands of the silica structure were seen at wavelengths of 1059 171 cm<sup>-1</sup> [46], 1053 cm<sup>-1</sup> [47], 1065 cm<sup>-1</sup> [15], and 1064 cm<sup>-1</sup> [48], respectively (**Fig. 2** (a)). The 172 bands of MCM-41 at 965 and 789 cm<sup>-1</sup> correspond to the Si-OH and Si-O structures, 173 respectively (Fig. 2 (a)) [49]. In addition, the peaks at 2927 cm<sup>-1</sup> and 2857 cm<sup>-1</sup> belong to the 174 expansion of the CH(CH<sub>2</sub>CH<sub>2</sub>CH<sub>2</sub>NH<sub>2</sub>) structure of MCM-48 (Fig. 2 (a)) [46]. -OH stretch can 175 be seen at the 1635 cm<sup>-1</sup> band and the water in the structure shows a wide bandgap of around 176 3368 cm<sup>-1</sup> (especially for MCM-41 and MCM-48; Fig. 2 (a)) [50]. The symmetrical stretching 177 vibration mode of O-H of isolated central silanol (Si-OH) groups are represented by the peaks 178 at 3725 cm<sup>-1</sup> (SBA-15; Fig. 2 (a)) and 3749 cm<sup>-1</sup> (MCM-48; Fig. 2 (a)) [50,51]. Although shifts 179 were observed in the Bragg fundamental peaks from the XRD analysis result of MCM-41, the 180 basic Bragg peaks of d(100), d(110), and d(200) reflections were obtained. These baseline 181 Bragg peak values obtained showed that MCM-41 had a regular hexagonal structure (Fig. 2 182 **(b)**) [50]. 183

184 Due to the SiO<sub>2</sub> groups in the structures of silica-based materials (MCM-41, MCM-48, SBA-185 15, and SBA-16), no clear differences may be observed in the FTIR results. In addition, precise determinations may not be possible due to the wide peaks of OH and Si-O-Si structures. After
the modification processes, clear differences can be observed in the FT-IR analysis results
depending on the functional groups. A more narrow wavelength result for the FT-IR analyses
are also given in Fig. S7 and S8 to emphasize some of the peaks in Fig. 2 (a).

190 MCM-48's main Bragg peaks (d(211) and d(220)) were measured at 20:1.33 and 2.4,

respectively (**Fig. 2** (**b**)) [42,46]. Low-angle XRD analysis showed that the main Bragg peak

192 (d110) of the SBA-16 support material was obtained at 20:0.84 (Fig. 2 (b)) [15,41]. XRD

analysis for SBA-15 showed that d(100) and d(110) reflections were observed showing the

194 main Bragg peaks of the mesoporous structure (**Fig. 2** (**b**)) [52].

According to the SEM analysis results, the cubic structure of MCM-48 [53], the hexagonal 195 structure of MCM-41 [53], the spherical structure of SBA-16 [15], and the wheat chain 196 structures of SBA-15 [54] were confirmed (Fig 2 (c)). Moreover, the EDX and MAPPING 197 analysis were used to determine the distributions of C and Si elements in the structure (Figures 198 S1-4). The SEM image of GO shows the randomly aggregated and crumpled sheets align with 199 the previously reported characteristics [55]. Finally, the surface characteristics of the 200 GO:MCM-41 composite were confirmed with SEM images demonstrating the crumbled GO 201 sheets were wrapped around the hexagonal structure of MCM-41. Thereby, the MCM-41 202 203 particles are shown to be covered with GO flakes that would provide electrical conductivity for 204 the prepared films (further confirmed by electrochemical measurements).

205

206





207

С

Fig. 2. (a) FT-IR analysis (b) low-angle XRD patterns and (c) SEM images of MCM-41, MCM-208

48, SBA-15, SBA-16, GO and GO:MCM-41 209

210

3.2. Electrochemical characterization and optimization of GO-mesoporous silica ratio 211 To investigate the behaviour of the GO-mesoporous silica-coated SPEs at different material 212 ratios, a series of CV experiments have been conducted in 0.1 M KCl containing 2 mM 213

K<sub>3</sub>Fe(CN)<sub>6</sub>/K<sub>4</sub>Fe(CN)<sub>6</sub>. Fig. 3 shows the voltammograms and respective anodic and cathodic
 peak current values with changing GO-mesoporous silica ratio.



216

**Fig. 3.** CVs (50 mV/s) and anodic and cathodic peak current values of (a) SPE/GO:MCM-41, (b) SPE/GO:MCM-48, (c) SPE/GO:SBA-15, (d) SPE/GO:SBA-16 in 2 mM  $K_3Fe(CN)_6/K_4Fe(CN)_6$  redox couple in 0.1 M KCl, (N= 3 samples).

A reversible redox response was observed for BE at ca. 0.18 V and ca. 0.075 V (vs Ag/Ag<sup>+</sup>) for oxidation and reduction processes, respectively. The voltage separation between anodic and cathodic peaks was ca. 0.1 V (vs Ag/Ag<sup>+</sup>) and the anodic to cathodic peak current ratio  $(i_{pa}/i_{pc})$ was ca. 1.02 suggesting chemical reversibility and quasi-reversible electron transfer [56]. It can also be seen that the modification of SPEs with GO and GO-MSM at different ratios didn't cause a significant difference in the electrochemical parameters.. However, different modifications on SPEs made a difference in the catalytic response between electrodes. GOmodified electrode (SPE/GO) showed a significant increase in anodic and cathodic peak current values showing higher peak current values than BE. On the other hand, electrodes modified with the silica materials for all mixing ratios showed lower peak current values than SPE/GO as the integration of electrically insulating silica with GO would be expected the lower the overall conductivity of the composite [57]. However, GO:MCM-41 modified electrode with a 1:1 ratio was the only configuration that resulted in the highest current values. As the pore volume and active surface area of the mesoporous silica increase, the interactions between GO and the silica material would change as well as the electrochemical response due to an increase in total electroactive area. MCM-41 was reported to have a relatively larger surface area and pore-loading capacity than other silica materials used in this study which could be the reason for the better response [40].

#### 3.3. Electrochemical glucose oxidation studies

After the electrochemical investigation of the GO-mesoporous silica materials, enzyme adsorption was performed to evaluate the performance of these compositions in enzymatic glucose oxidation. In this work, the molecular aspects of mesoporous silica materials were not taken into account in the performance of the enzymatic performance, rather it was aimed to compare the performance of the different types of silica materials in the performance of enzymatic glucose oxidation. Therefore a series of CA experiments were performed in 0.1 PBS solution containing 1 mM FcCOOH as an electron transfer mediator. FcCOOH was chosen as a reliable electron transfer mediator in aqueous electrochemistry that was widely used in the literature [58,59]. The optimization studies for enzyme concentration using LSV revealed that increasing the enzyme concentration for immobilization didn't cause a significant change in the performance of electrochemical glucose oxidation (**Fig. S5**). This could be due to the saturation that might be reached in the mesopores of the silica materials, hence further increasing the enzyme concentration wouldn't make a significant contribution to the catalytic response due to mass transfer limitations. As a result, 1 mg/mL was chosen for the electrochemical

experiments. After enzyme loading optimization, CA experiments were performed using modified SPEs with GO, GO:MCM-41, GO:MCM-48, GO:SBA-15, and GO:SBA-16 with a material loading of 0.15 mg/cm<sup>2</sup> at a 1:1 ratio to investigate the analytical performance of the prepared electrodes. Fig. 4 shows the CA response of SPE/GO/GOx, SPE/GO:MCM-41/GOx, and SPE/GO:MCM-48/GOx with increasing glucose concentration. SPE/GO:SBA-15/GOx and SPE/GO:SBA-16/GOx electrodes were also tested but didn't show a linear response (Fig. S6). However, MCM-modified electrodes showed a relatively good response to different glucose concentrations up to 7 mM. SPE/GO:MCM-41/GOx showed the best performance among all silica-modified electrodes showing similar performance to GO-only electrodes. In terms of analytical performance the sensitivity of GO, GO:MCM-41, and GO:MCM-48-modified electrodes were calculated as 0.51 µA/mM, 0.39 µA/mM, and 0.17 µA/mM, respectively. These suggest that MCM-modified electrodes showed promising performance compared to other GO-modified electrodes without giving up a significant analytical performance similar to previous investigations without the incorporation of the enzyme. On the other hand, although this study didn't aim to develop a functional enzymatic biosensor, the following limit of detection (LOD) values were calculated for GO, GO:MCM-41, and GO:MCM-48-modified electrodes as 0.43, 2.62, and 0.80 mM, respectively (LOD: 3.3xSD/Slope) [60].



**Fig. 4.** CA curves (applied voltage: 0.14 V for 120 s) and calibration graphs of (**a**) and (**d**) SPE/GO, (**b**) and (**e**) SPE/GO:MCM-41, and (**c**) and (**d**) SPE/GO:MCM-48 electrodes tested in 0.1 M PBS (pH 7.4) containing 1 mM FcCOOH for glucose concentrations between 0 and 7 mM, (N= 3 samples).

Enzyme-modified electrodes usually suffer from low stability in vitro and significant effort has been spent to improve the stability of enzymes immobilized on electrodes [61,62]. In this study, silica was used to help enhance enzyme stability, therefore, a series of inter-day and intra-day experiments have been performed. The anodic peak current values of the LSV experiments were used to investigate the stability of the enzyme immobilized on different modified electrodes. The tests were conducted with SPE/GO/GOx and SPE/GO:MCM-41/GOx electrodes in 0.1 M PBS containing 1 mM FcCOOH and glucose concentrations of 0 and 5 mM.



**Fig. 5.** Intraday (**a**) and interday (**b**) stability experiments of SPE/GO and SPE/GO:MCM-41 electrodes for 0 and 5 mM glucose concentrations. Electrodes were tested in 0.1 M PBS (pH 7.4) containing 1 mM FcCOOH, (N= 3 samples).

**Fig. 5 (a)** shows the intraday experiment results consisting of 6 measurements with 1 h intervals. The electrodes were kept in 0.1 M PBS between experiments at room temperature for intraday and +4°C for interday experiments and washed with 0.1 PBS before tests. The intraday experimental results show that both electrodes show similar performance, and the results didn't show a significant change in the current response regardless of glucose concentration. On the other hand, interday experiments for 14 days (tested on days 0, 7, and 14) revealed that the performance of the SPE/GO:MCM41/GOx electrode showed superior performance over the SPE/GO/GOx electrode (**Fig. 5 (b**)). **Table 1** also summarizes the percentage change for intraday and interday stability measurements. The SPE/GO/GOx electrode showed a 40.57% decrease in current whereas the current change for SPE/GO:MCM-41/GOx was ca. 13.75%. All intraday and interday experiments showed a good degree of repeatability with relative standard deviation (RSD %) values less than 10% except for SPE/GO/GOx electrode compared to

SPE/GO:MCM-41/GOx supporting that silica-based GO composite might provide a more suitable environment for coating and enzyme stability. The RSD values of the intraday and interday stability experiments are presented in **Table S1**.

Electrode	Intraday stability % change		Interday* stability % change	
Configuration	0 mM	5 mM	0 mM	5 mM
GO	1.45	10.95	4.83	40.57
GO/MCM-41	7.36	17.32	1.61	13.75

Table 1. Percentage change for inter-day and intra-day stability experiments

\* Tested on days 0, 7 and 14.

#### 4. Conclusion

In this study, an electrochemical investigation of the performance of different GO composite materials prepared using mesoporous silica materials (MCM-41, MCM-48, SBA-15, and SBA-16) on enzymatic glucose oxidation. Optimization studies were conducted to find the optimal GO-to-mesoporous silica ratio and the effect of enzyme loading on the performance of the prepared electrodes. The results showed that the GO to mesoporous silica ratio was found to be 1:1 and the optimum enzyme working concentration was 1 mg/mL. Among all mesoporous silica materials, MCM:41 showed the most promising performance, therefore it was used for the enzymatic investigations. Enzymatic glucose oxidation experiments showed that GO:MCM-41-modified electrodes showed very promising results in detecting different glucose levels at similar sensitivity values. The sensitivity of enzyme-immobilized GO, GO:MCM-41, and GO:MCM-48-modified electrodes were calculated as 0.51 µA/mM, 0.39 µA/mM, and 0.17 µA/mM, respectively. Furthermore, it showed superior stability compared to GO-only modified enzymatic electrodes. Interday experiments revealed that SPE/GO/GOx electrode showed a 40% decrease in current whereas the current change for SPE/GO:MCM- 41/GOx was about 14%. This study shows that an optimized amount of composite materials (1:1 for this study) consisting of GO and mesoporous silica, especially MCM-41 due to its relatively larger surface area and pore-loading capacity, can provide a suitable environment for enzyme retention on the surface. These findings could be important for long-term applications of enzymes such as enzymatic biofuel cells and continuous monitoring of glucose where the stability of the enzymes on silica supports such as MCM-family is one of the key factors for the desired performance.

#### Acknowledgements

The authors state that there is no conflict of interest. We would like to thank the Scientific Research Council of Bilecik Seyh Edebali University (BAP), Project no: 2018-02.BŞEÜ.03-09, for financial support. This study also includes a part of Ms. Şevval Kaya's M.Sc. thesis.

## References

1. Hoffmann F, Cornelius M, Morell J, Fröba M (2006) Silica-based mesoporous organicinorganic hybrid materials. Angew Chem, Int Ed 45 (20):3216-3251

2. Tang F, Li L, Chen D (2012) Mesoporous silica nanoparticles: synthesis, biocompatibility and drug delivery. Adv Mater 24 (12):1504-1534

3. Etienne M, Zhang L, Vilà N, Walcarius A (2015) Mesoporous Materials-Based Electrochemical Enzymatic Biosensors. Electroanalysis 27 (9):2028-2054

4. Walcarius A (2018) Silica-based electrochemical sensors and biosensors: Recent trends. Curr Opin Electrochem 10:88-97

5. Øye G, Sjöblom J, Stöcker MJAic, science i (2001) Synthesis, characterization and potential applications of new materials in the mesoporous range. 89:439-466

6. Yang Z, Lu Y, Yang ZJCc (2009) Mesoporous materials: tunable structure, morphology and composition. (17):2270-2277

7. Martínez-Carmona M, Gun'ko YK, Vallet-Regí MJP (2018) Mesoporous silica materials as drug delivery:"The Nightmare" of bacterial infection. 10 (4):279

8. Zhao D, Huo Q, Feng J, Chmelka BF, Stucky GD (1998) Nonionic triblock and star diblock copolymer and oligomeric surfactant syntheses of highly ordered, hydrothermally stable, mesoporous silica structures. J Am Chem Soc 120 (24):6024-6036

9. Bachari K, Guerroudj R, Lamouchi MJAJoC (2017) Catalytic behavior of gallium-containing mesoporous silicas. 10:S301-S305

10. Ouargli R, Hamacha R, Benharrats N, Boos A, Bengueddach AJJoPM (2015)  $\beta$ -diketone functionalized SBA-15 and SBA-16 for rapid liquid–solid extraction of copper. 22:511-520

11. Tu J, Wang R, Geng W, Lai X, Zhang T, Li N, Yue N, Li XJS, Chemical AB (2009) Humidity sensitive property of Li-doped 3D periodic mesoporous silica SBA-16. 136 (2):392-398

12. Boukoussa B, Hamacha R, Morsli A, Bengueddach AJAJoC (2017) Adsorption of yellow dye on calcined or uncalcined Al-MCM-41 mesoporous materials. 10:S2160-S2169

13. Chen C-Y, Li H-X, Davis ME (1993) Studies on mesoporous materials: I. Synthesis and characterization of MCM-41. Microporous Mater 2 (1):17-26

14. Alfredsson V, Anderson MW (1996) Structure of MCM-48 revealed by transmission electron microscopy. Chem Mater 8 (5):1141-1146

15. Cao Z, Du P, Duan A, Guo R, Zhao Z, lei Zhang H, Zheng P, Xu C, Chen Z (2016) Synthesis of mesoporous materials SBA-16 with different morphologies and their application in dibenzothiophene hydrodesulfurization. Chem Eng Sci 155:141-152

16. Campanati M, Fornasari G, Vaccari A (2003) Fundamentals in the preparation of heterogeneous catalysts. Catal Today 77 (4):299-314

17. Walcarius A, Mandler D, Cox JA, Collinson M, Lev O (2005) Exciting new directions in the intersection of functionalized sol–gel materials with electrochemistry. J Mater Chem 15 (35-36):3663-3689

 Yang X, Qiu P, Yang J, Fan Y, Wang L, Jiang W, Cheng X, Deng Y, Luo W (2021) Mesoporous materials-based electrochemical biosensors from enzymatic to nonenzymatic. Small 17 (9):1904022

19. Zhi J, Wang Y, Deng S, Hu AJRA (2014) Study on the relation between pore size and supercapacitance in mesoporous carbon electrodes with silica-supported carbon nanomembranes. 4 (76):40296-40300

20. Yang X, Li Z, Zhi J, Ma J, Hu AJL (2010) Synthesis of ultrathin mesoporous carbon through Bergman cyclization of enediyne self-assembled monolayers in SBA-15. 26 (13):11244-11248

21. Fang Y, Hu Q, Yu X, Wang L (2018) Ultrasensitive electrochemical immunosensor for procalcitonin with signal enhancement based on zinc nanoparticles functionalized ordered mesoporous carbon-silica nanocomposites. Sens Actuators, B 258:238-245

22. Kordasht HK, Pazhuhi M, Pashazadeh-Panahi P, Hasanzadeh M, Shadjou N (2020) Multifunctional aptasensors based on mesoporous silica nanoparticles as an efficient platform for bioanalytical applications: Recent advances. TrAC, Trends Anal Chem 124:115778

23. Zhou G, Fung KK, Wong LW, Chen Y, Renneberg R, Yang S (2011) Immobilization of glucose oxidase on rod-like and vesicle-like mesoporous silica for enhancing current responses of glucose biosensors. Talanta 84 (3):659-665

24. Carlsson N, Gustafsson H, Thörn C, Olsson L, Holmberg K, Åkerman B (2014) Enzymes immobilized in mesoporous silica: a physical–chemical perspective. Adv Colloid Interface Sci 205:339-360

25. Magner E (2013) Immobilisation of enzymes on mesoporous silicate materials. Chem Soc Rev 42 (15):6213-6222

26. Zhang J, Chen S, Tan X, Zhong X, Yuan D, Cheng Y (2014) Highly sensitive electrochemiluminescence biosensors for cholesterol detection based on mesoporous magnetic core–shell microspheres. Biotechnol Lett 36:1835-1841

27. Xu X, Lu P, Zhou Y, Zhao Z, Guo M (2009) Laccase immobilized on methylene blue modified mesoporous silica MCM-41/PVA. Mater Sci Eng C 29 (7):2160-2164

28. Zhou M, Shang L, Li B, Huang L, Dong S (2008) Highly ordered mesoporous carbons as electrode material for the construction of electrochemical dehydrogenase-and oxidase-based biosensors. Biosens Bioelectron 24 (3):442-447

29. Fang ZH, Lu LM, Zhang XB, Li HB, Yang B, Shen GL, Yu RQ (2011) A Third-Generation Hydrogen Peroxide Biosensor Based on Horseradish Peroxidase Immobilized in Carbon Nanotubes/SBA-15 Film. Electroanalysis 23 (10):2415-2420

30. Shimomura T, Sumiya T, Ono M, Itoh T, Hanaoka T-a (2012) An electrochemical biosensor for the determination of lactic acid in expiration. Procedia Chem 6:46-51

31. Mundaca-Uribe R, Bustos-Ramírez F, Zaror-Zaror C, Aranda-Bustos M, Neira-Hinojosa J, Pena-Farfal C (2014) Development of a bienzymatic amperometric biosensor to determine uric acid in human serum, based on mesoporous silica (MCM-41) for enzyme immobilization. Sens Actuators, B 195:58-62

32. Bai Y, Yang H, Yang W, Li Y, Sun C (2007) Gold nanoparticles-mesoporous silica composite used as an enzyme immobilization matrix for amperometric glucose biosensor construction. Sens Actuators, B 124 (1):179-186

33. Zhang J, Zhu J (2009) A novel amperometric biosensor based on gold nanoparticlesmesoporous silica composite for biosensing glucose. Sci China, Ser B: Chem 52 (6):815-820

34. Lai G, Zhang H, Yu A, Ju H (2015) In situ deposition of Prussian blue on mesoporous carbon nanosphere for sensitive electrochemical immunoassay. Biosens Bioelectron 74:660-665

35. Wang K, Yang H, Zhu L, Liao J, Lu T, Xing W, Xing S, Lv Q (2009) Direct electrochemistry and electrocatalysis of glucose oxidase immobilized on glassy carbon electrode modified by Nafion and ordered mesoporous silica-SBA-15. J Mol Catal B: Enzym 58 (1-4):194-198

36. Caro-Jara N, Mundaca-Uribe R, Zaror-Zaror C, Carpinelli-Pavisic J, Aranda-Bustos M, Peña-Farfal C (2013) Development of a Bienzymatic Amperometric Glucose Biosensor Using Mesoporous Silica (MCM-41) for Enzyme Immobilization and Its Application on Liquid Pharmaceutical Formulations. Electroanalysis 25 (1):308-315

37. Boujakhrout A, Sánchez E, Díez P, Sánchez A, Martínez-Ruiz P, Parrado C, Pingarrón JM, Villalonga R (2015) Single-Walled Carbon Nanotubes/Au–Mesoporous Silica Janus Nanoparticles as Building Blocks for the Preparation of a Bienzyme Biosensor. ChemElectroChem 2 (11):1735-1741

38. Yusan S, Rahman MM, Mohamad N, Arrif TM, Latif AZA, MA MA, Wan Nik WSBJJoamic (2018) Development of an amperometric glucose biosensor based on the immobilization of glucose oxidase on the Se-MCM-41 mesoporous composite. 2018

39. Tvorynska S, Barek J, Josypcuk BJB (2022) Influence of different covalent immobilization protocols on electroanalytical performance of laccase-based biosensors. 148:108223

40. Şimşek V (2019) Investigation of catalytic sustainability of silica-based mesoporous acidic catalysts and ion-exchange resins in methyl acetate synthesis and characterizations of synthesized catalysts. Arabian J Sci Eng 44 (6):5301-5310

41. Veli S, Pinar A (2018) Characterization and catalytic performance of modified sba-16 in liquid phase reaction. Int J Chem React Eng 16 (8)

42. Li H, Wang S, Ling F, Li J (2006) Studies on MCM-48 supported cobalt catalyst for Fischer–Tropsch synthesis. J Mol Catal A: Chem 244 (1-2):33-40

43. Şimşek V, Şahin S (2019) Characterization and catalytic performance evaluation of a novel heterogeneous mesoporous catalyst for methanol–acetic acid esterification. J Porous Mater 26:1657-1665

44. Şahin S, Kaya Ş, Üstündağ Z, Caglayan MOJJoSSE (2022) An electrochemical signal switch–based (on–off) aptasensor for sensitive detection of insulin on gold-deposited screen-printed electrodes. 26 (4):907-915

45. Şahin S (2020) A simple and sensitive hydrogen peroxide detection with horseradish peroxidase immobilized on pyrene modified acid-treated single-walled carbon nanotubes. J Chem Technol Biotechnol 95 (4):1093-1099

46. Huang HY, Yang RT, Chinn D, Munson CL (2003) Amine-grafted MCM-48 and silica xerogel as superior sorbents for acidic gas removal from natural gas. Ind Eng Chem Res 42 (12):2427-2433

47. Nasiriani T, Nazeri MT, Shaabani A (2023) Cobalt phthalocyanine conjugated SBA-15 mesoporous silica via the Ugi four-component reaction: A potential heterogeneous catalytic nanocomposite for CO2 fixation reaction. Microporous Mesoporous Mater:112514

48. Saikia L, Srinivas D, Ratnasamy P (2007) Comparative catalytic activity of Mn (Salen) complexes grafted on SBA-15 functionalized with amine, thiol and sulfonic acid groups for selective aerial oxidation of limonene. Microporous Mesoporous Mater 104 (1-3):225-235

49. Colilla M, Izquierdo-Barba I, Sánchez-Salcedo S, Fierro JL, Hueso JL, Vallet-Regí Ma (2010) Synthesis and characterization of zwitterionic SBA-15 nanostructured materials. Chem Mater 22 (23):6459-6466

50. Bhagiyalakshmi M, Yun LJ, Anuradha R, Jang HT (2010) Synthesis of chloropropylamine grafted mesoporous MCM-41, MCM-48 and SBA-15 from rice husk ash: their application to CO 2 chemisorption. J Porous Mater 17:475-484

51. Mirji S, Halligudi S, Mathew N, Jacob NE, Patil K, Gaikwad A (2007) Adsorption of methanol on mesoporous SBA-15. Mater Lett 61 (1):88-92

52. Liu Q-Y, Wu W-L, Wang J, Ren X-Q, Wang Y-R (2004) Characterization of 12tungstophosphoric acid impregnated on mesoporous silica SBA-15 and its catalytic performance in isopropylation of naphthalene with isopropanol. Microporous Mesoporous Mater 76 (1-3):51-60 53. Schumacher K, Ravikovitch PI, Du Chesne A, Neimark AV, Unger KK (2000) Characterization of MCM-48 materials. Langmuir 16 (10):4648-4654

54. Sayari A, Han B-H, Yang Y (2004) Simple synthesis route to monodispersed SBA-15 silica rods. J Am Chem Soc 126 (44):14348-14349

55. Stankovich S, Dikin DA, Piner RD, Kohlhaas KA, Kleinhammes A, Jia Y, Wu Y, Nguyen ST, Ruoff RS (2007) Synthesis of graphene-based nanosheets via chemical reduction of exfoliated graphite oxide. carbon 45 (7):1558-1565

56. Elgrishi N, Rountree KJ, McCarthy BD, Rountree ES, Eisenhart TT, Dempsey JL (2018) A practical beginner's guide to cyclic voltammetry. J Chem Educ 95 (2):197-206

57. Shen C, Wang H, Zhang T, Zeng Y (2019) Silica coating onto graphene for improving thermal conductivity and electrical insulation of graphene/polydimethylsiloxane nanocomposites. J Mater Sci Technol 35 (1):36-43

58. Sahin S, Wongnateb T, Chaiyenb P, Yu EH (2014) Glucose oxidation using oxygen resistant pyranose-2-oxidase for biofuel cell applications. Chem Eng Trans 41

59. Chaubey A, Malhotra B (2002) Mediated biosensors. Biosens Bioelectron 17 (6-7):441-456

60. Lister AS (2005) Validation of HPLC methods in pharmaceutical analysis. In: Separation Science and Technology, vol 6. Elsevier, pp 191-217

61. Sassolas A, Blum LJ, Leca-Bouvier BD (2012) Immobilization strategies to develop enzymatic biosensors. Biotechnol Adv 30 (3):489-511

62. Xiao X, Xia H-q, Wu R, Bai L, Yan L, Magner E, Cosnier S, Lojou E, Zhu Z, Liu A (2019) Tackling the challenges of enzymatic (bio) fuel cells. Chem Rev 119 (16):9509-9558